AMENDMENTS TO THE SPECIFICATION:

Please replace the paragraph that begins on page 3, line 9, with the following paragraph:

> Local administration of therapeutic agents via stents has shown ~~some~~ favorable results in reducing restenosis. However, there is a great need for better and more effective coatings for ~~the~~ local drug delivery.

Please replace the paragraph that begins on page 4, line 6, with the following paragraph:

> A medical article comprising an implantable substrate having a coating is provided[[,]]; the coating includes phosphoryl choline or polyaspirin.

Please replace the paragraph that begins on page 4, line 8, with the following paragraph:

> A method for fabricating a medical article is provided[[, the]]. The method includes applying a coating ~~on~~ to at least a portion of an implantable substrate, the coating including an ABA or an AB block copolymer, wherein one of the moieties in the block copolymer produces a biological response and the other moiety provides the block copolymer with structural functionality.

Please replace the paragraph that begins on page 5, line 15, with the following paragraph:

> "Fast release" is defined as *in vivo* release of substantially the entire amount of the drug from the stent coating in less than 15 days, for example, within 7 to 14 days. "Slow release" is defined as *in vivo* release of substantially the entire amount of the drug from the stent coating in 15 days or longer, for example, within 15 to 56 days.

Please replace the paragraph that begins on page 6, line 7, with the following paragraph:

> A coating for an implantable medical device, such as a stent, according to embodiments of the present invention, can be a multi-layer structure that can include the following four layers:
>
> (a) a drug-polymer layer (also referred to as "reservoir" or "reservoir layer") or ~~alternatively~~ a polymer-free drug layer;
>
> (b) an optional primer layer;
>
> (c) an optional topcoat layer; and/or
>
> (d) an optional finishing coat layer.

Please replace the paragraph that begins on page 7, line 15, with the following paragraph:

> The drug-polymer layer can be applied directly onto at least a part of the stent surface to serve as a reservoir for at least one active agent or a drug, which is incorporated into the reservoir layer. The optional primer layer can be applied between the stent and the reservoir to improve the adhesion of the drug-polymer layer to the stent. The optional topcoat layer can be applied over at least a portion of the reservoir layer and serves as a rate limiting membrane, which helps to control the rate of release of the drug. In one embodiment, the topcoat layer can be essentially free from any active agents or drugs. In another embodiment, besides the active agent or drug contained in the reservoir layer, the topcoat can incorporate an additional active agent or drug, for example, by having the additional drug or active agent conjugated to the polymer forming the topcoat layer. If ~~the~~ a topcoat layer is used, the optional finishing coat layer can be applied over at least a portion of the topcoat layer for improving the biocompatibility of the coating.

Please replace the paragraph that begins on page 8, line 13, with the following paragraph:

> In one embodiment, any or all of the layers of the stent coating[[,]] can be made of a polymer that is[[both]] biologically beneficial and biologically degradable, erodable, absorbable, and/or resorbable. In another embodiment, the outermost layer of the coating can be limited to such a polymer.

Please replace the paragraph that begins on page 8, line 17, with the following paragraph:

> To illustrate in more detail, in the stent coating having all four layers described above (i.e., the primer, the reservoir layer, the topcoat layer and the finishing coat layer), the outermost layer is the finishing coat layer, which is made of a polymer that is[[both]] biologically beneficial and biologically degradable, erodable, absorbable, and/or resorbable. In this case, optionally, the remaining layers (i.e., the primer, the reservoir layer, the topcoat layer) can also be[[also]] fabricated ~~of~~ from a polymer that is[[both]] biologically beneficial and biologically degradable; [[and]]the polymer can be the same or different in each layer.

Please replace the paragraph that begins on page 9, line 14, with the following paragraph:

> The biological degradation, erosion, absorption and/or resorption of a biologically degradable, erodable, absorbable and /or resorbable and biologically beneficial polymer are expected to cause at least three results. First, the rate of release of the drug will increase due to the gradual disappearance of the polymer that forms the reservoir or the topcoat layer, or both. By choosing an appropriate degradable ~~polymer~~ polymer, the stent coating can be engineered to provide either fast or slow release of the drug, as desired. Those having ordinary skill in the art can determine whether a stent coating having slow or fast release is advisable for a particular drug. For example, fast release may be recommended for stent coatings loaded with antimigratory ~~drugs~~ drugs, which often need to be released within 1 to 2

weeks. For antiproliferative drugs, slow release may be needed (up to 30 days release time).

Please replace the paragraph that begins on page 10, line 8, with the following paragraph:

Third, ~~when~~ upon degradation of a biologically degradable, erodable, absorbable and/or resorbable polymer, which is at the same time[[is]] biologically beneficial~~, degrades~~, the products of degradation of the polymer can serve as[[yet]] other additional active agents ~~which~~ which, can be absorbed by the body of the patient bringing about additional medical and biological benefits.

Please replace the paragraph that begins on page 10, line 12, with the following paragraph:

Biologically degradable, erodable, absorbable and /or resorbable polymers ~~which~~ that are also biologically beneficial~~, that~~ and that can be used for making any of the stent coating ~~layers~~ layers, include block copolymers. Examples of block copolymers include ~~such as~~ ABA ~~block copolymers;~~block copolymers, AB block copolymers~~;~~, or polymers ~~which~~ that are not necessarily block copolymers, as defined below, but still comprise ABA or AB blocks. Both ABA and AB ~~block copolymers~~block copolymers contain a polymeric moiety A and a polymeric moiety B.

Please replace the paragraph that begins on page 10, line 18, with the following paragraph:

One way of describing the ABA ~~block copolymers can be~~ block copolymers is by using the formula $[–A–A–A]_m–[B–B–B]_n–[A–A–A]_p–$, where each of "m," "n," and "p" is an integer greater than 0. The AB ~~block copolymers~~ block-copolymers can be described by the formula $[–A–A–A]_m–[B–B–B–]_n$, where each of "m" and "n[[,]]" is an integer greater than 0. The blocks of the ABA and AB block copolymers need not be linked on the ends, since the values of the integers determining the number of A and B blocks ~~are such as to~~ ensure that the individual blocks are usually

long enough to be considered polymers in their own right. Accordingly, the ABA block copolymer can be named ~~poly A-block-co-poly B-block-co-poly A-block copolymer~~ poly-A-block-co-poly-B-block-co-poly-A-block copolymer, and the AB block copolymer can be named ~~poly A-block-co-poly B-block copolymer~~ poly-A-block-co-poly-B-block copolymer. Blocks "A" and "B," typically[[,]] larger than three-block size, can be alternating or random. The values of "m" and "p" can be selected ~~so as~~ to have the block co-polymer with the molecular weight of blocks A between about 300 and about 40,000 Daltons, such as between about 8,000 and about 30,000 Daltons, for example, about 15,000 Daltons. The values of "n" are selected ~~so as~~ to have the block copolymer with the molecular weight of blocks B between about 50,000 and about 250,000 Daltons, such as between about 80,000 and about 200,000 Daltons, for example, about 100,000 Daltons.

Please replace the paragraph that begins on page 11, line 11, with the following paragraph:

In the ABA and AB block copolymers, one polymeric moiety can provide the ~~block copolymer~~ block copolymer with blood compatibility ("a biocompatible moiety")[[,]] and the other polymeric moiety ("a structural moiety") can provide the ~~block copolymer~~ block copolymer with mechanical and adhesive properties that the ~~block copolymer~~ block co-polymer needs ~~to have to be suitable~~ for making the stent coatings. In one embodiment, moiety A is the biocompatible moiety[[,]] and moiety B is the structural moiety. In another embodiment, moiety A is the structural moiety[[,]] and moiety B is the biocompatible moiety. The biocompatible and the structural moieties are selected ~~so that~~ to make the ABA and AB block-copolymers biologically degradable. Examples of suitable biocompatible moieties include poly(alkylene glycols), for example, poly(ethylene glycol) (PEG), poly(ethylene oxide), poly(propylene glycol) (PPG), poly(tetramethylene glycol), poly(ethylene oxide-co-propylene oxide), poly(N-vinyl pyrrolidone), poly(acrylamide methyl propane sulfonic acid) and salts thereof (AMPS and salts thereof), poly(styrene sulfonate), sulfonated dextran, polyphosphazenes, poly(orthoesters), poly(tyrosine carbonate), hyaluronic acid, hyaluronic acid having a stearoyl or palmitoyl substitutent group, copoly-

mers of PEG with hyaluronic acid or with hyaluronic acid-stearoyl, or with hyaluronic acid-palmitoyl, heparin, co-polymers of PEG with heparin, a graft copolymer of poly(L-lysine) and PEG, or copolymers thereof. A molecular weight of a suitable biocompatible polymeric moiety can be below 40,000 Daltons to ensure the renal clearance of the compound, for example, between about 300 and about 40,000 Daltons, more narrowly, between about 8,000 and about 30,000 Daltons, for example, about 15,000 Daltons.

Please replace the paragraph that begins on page 12, line 8, with the following paragraph:

Examples of suitable structural moieties include poly(caprolactone) (PCL), poly(butylene terephthalate) (PBT), poly(ester amide), moieties containing butyl methacrylate fragments, moieties containing a lauryl group, poly(lactic acid)(PLA), poly(aspirin[[e]]), and copolymers thereof. Molecular weight of the blocks comprising the structural moiety can be between about 20,000 and about 250,000 Daltons, more narrowly, between about 80,000 and about 200,000 Daltons, such as about 100,000 Daltons.

Please replace the paragraph that begins on page 12, line 14, with the following paragraph:

One example of the biodegradable ABA block copolymer is poly(~~ethylene~~ ethylene glycol)-block-poly(caprolactone)-block-poly(~~ethylene~~ ethylene glycol)(PEG-PCL-PEG). One possible structure of the PEG-PCL-PEG block co-polymer is shown by formula (I):

Please replace the paragraph that begins on page 12, line 21, with the following paragraph:

In the PEG-PCL-PEG block copolymers shown by formula (I), the PEG blocks constitute the biodegradable moiety, while the PCL block constitutes the structural moiety. If desired, the positions of the moieties can be switched to obtain a BAB block copolymer, poly(caprolactone)-block-

poly(~~ethylene~~ ethylene glycol)-block poly(caprolactone)(PCL-PEG-PCL). One possible structure of the PCL-PEG-PCL block copolymer is shown by formula (II):

Please replace the paragraph that begins on page 13, line 5, with the following paragraph:

Block copolymers shown by formulae (I) and (II) can be synthesized by standard methods known to those having ordinary skill in the art, for example, by acid- or based-catalyzed copolycondensation of PEG with PCL. Another example of ~~the~~ a PEG-containing polyester, suitable for making a stent and/or a stent coating in accordance with the present invention includes a block-copolymer of PEG with PBT, such as poly(~~ethylene~~ ethylene glycol)-block-poly(butyleneterephthalate) (PEG-PBT), poly(~~ethylene~~ ethylene glycol)-block-poly (butylene terephthalate)-block-poly(~~ethylene~~ ethylene glycol) (PEG-PBT-PEG). PEG-PBT-PEG block-copolymer can be obtained, for example, by trans-esterification of dibutyleneterephthalate with PEG. Another example of the PEG-containing polyester, suitable for making a stent and/or a stent coating in accordance with the present invention includes a block-copolymer of PEG with PLA, such as poly(~~ethylene~~ ethylene glycol)-block-poly (lactic acid)-block-poly(~~ethylene~~ ethylene glycol) (PEG-PLA-PEG). In PEG-PLA-PEG, the molecular weight of the units derived from ethylene glycol can be between about 550 and about 30,000 Daltons, and the molecular weight of the units derived from lactic acid can be between about 20,000 and about 150,000 Daltons.

Please replace the paragraph that begins on page 14, line 3, with the following paragraph:

Alternatively, if desired, the positions of the moieties in the PEG-PBT-PEG and PEG-PLA-PEG block copolymers can be switched to obtain a BAB block copolymers, poly(butyleneterephthalate)-block-poly(~~ethylene~~ ethylene glycol)-block poly(butyleneterephthalate) (PBT-PEG-PBT) and poly(lactic acid)-block-poly(ethylene glycol)-block-poly(lactic acid) (PLA-PEG-PLA).

Please replace the paragraph that begins on page 14, line 8, with the following paragraph:

> PEG-PCL-PEG , PCL-PEG-PCL, PEG-PBT, PEG-PBT-PEG, PBT-PEG-PBT, PEG-PLA-PEG and PLA-PEG-PLA block copolymers all contain fragments with ester bonds. Ester bonds are known to be water-labile bonds. When in contact with slightly alkaline blood, ester bonds are subject to catalyzed hydrolysis, thus ensuring biological degradability of the ~~block~~ block copolymer. One product of degradation of every block polymer, belonging to the group PEG-PCL-PEG , PCL-PEG-PCL, PEG-PBT, PEG-PBT-PEG, PBT-PEG-PBT, PEG-PLA-PEG and PLA-PEG-PLA is expected to be PEG, which is highly biologically compatible. PEG also has an additional advantage of being biologically beneficial, reducing smooth muscle cells proliferation at the lesion site and thus capable of inhibiting restenosis.

Please replace the paragraph that begins on page 14, line 17, with the following paragraph:

> In one embodiment, instead of, or in addition to, the ABA ~~block~~ block copolymers and/or AB block copolymers described above, compounds other than ABA ~~block~~ block copolymers and/or AB block copolymers can be used for making any layer of the stent coating, so long as these compounds are both biologically degradable and biologically beneficial. Examples of such compounds include polyaspirin and phosphoryl choline.

Please replace the paragraph that begins on page 14, line 22, with the following paragraph:

> Any layer of the stent coating can contain any amount of the biodegradable ABA or AB block copolymers described above, or a blend of more than one[[of]] such copolymers. If less than 100% of the layer is made of the biodegradable ABA or AB block copolymer(s), other~~, alternative,~~ polymers can comprise the balance. Examples of the alternative polymers that can be used include polyacrylates, such as poly(butyl methacrylate), poly(ethyl methacrylate), and

poly(ethyl methacrylate-co-butyl methacrylate), and fluorinated polymers and/or copolymers, such as poly(vinylidene fluoride) and poly(vinylidene fluoride-co-hexafluoro propene), poly(N-vinyl pyrrolidone), poly(hydroxyvalerate), poly(L-lactic acid), polycaprolactone, poly(lactide-co-glycolide), poly(hydroxybutyrate), poly(hydroxybutyrate-co-valerate), polydioxanone, polyorthoester, polyanhydride, poly(glycolic acid), poly(D,L-lactic acid), poly(glycolic acid-co-trimethylene carbonate), polyphosphoester, polyphosphoester urethane, poly(amino acids), cyanoacrylates, poly(trimethylene carbonate), poly(iminocarbonate), copoly(ether-esters), polyalkylene oxalates, polyphosphazenes, biomolecules (such as fibrin, fibrinogen, cellulose, starch, collagen and hyaluronic acid), polyurethanes, silicones, polyesters, polyolefins, polyisobutylene and ethylene-alphaolefin copolymers, vinyl halide polymers and copolymers (such as polyvinyl chloride), polyvinyl ethers (such as polyvinyl methyl ether), polyvinylidene chloride, polyacrylonitrile, polyvinyl ketones, polyvinyl aromatics (such as polystyrene), polyvinyl esters (such as polyvinyl acetate), copolymers of vinyl monomers with each other and olefins, e.g., poly(ethylene-co-vinyl alcohol) (EVAL), ethylene-methyl methacrylate copolymers, acrylonitrile-styrene copolymers, ABS resins, and ethylene-vinyl acetate copolymers; polyamides (such as Nylon 66 and polycaprolactam), alkyd resins, polycarbonates, polyoxymethylenes, polyimides, polyethers, epoxy resins, polyurethanes, rayon, rayon-triacetate, cellulose, cellulose acetate, cellulose butyrate, cellulose acetate butyrate, cellophane, cellulose nitrate, cellulose propionate, cellulose ethers, and carboxymethyl cellulose.

Please replace the paragraph that begins on page 16, line 1, with the following paragraph:

Representative examples of some solvents suitable for making the stent coatings include N,N-dimethylacetamide (DMAC), N,N-dimethylformamide (DMF), tethrahydrofuran[[e]] (THF), cyclohexanone, xylene, toluene, acetone, *i*-propanol, methyl ethyl ketone, propylene glycol monomethyl ether, methyl butyl ketone, ethyl acetate, *n*-butyl acetate, and dioxane. Some solvent mixtures can be ~~used~~ used, as well. Representative examples of the mixtures include:

(1) DMAC and methanol (e.g., a 50:50 by mass mixture);

(2) water, *i*-propanol, and DMAC (e.g., a 10:3:87 by mass mixture);

(3) *i*-propanol, and DMAC (e.g., 80:20, 50:50, or 20:80 by mass mixtures);

(4) acetone and cyclohexanone (e.g., 80:20, 50:50, or 20:80 by mass mixtures);

(5) acetone and xylene (e.g. a 50:50 by mass mixture);

(6) acetone, FLUX REMOVER AMS, and xylene (e.g., a 10:50:40 by mass mixture); and

(7) 1,1,2-trichloroethane and chloroform (e.g., ~~a~~ an 80:20 by mass mixture).

Please replace the paragraph that begins on page 16, line 15, with the following paragraph:

FLUX REMOVER AMS is trade name of a solvent manufactured by Tech Spray, Inc. of Amarillo, Texas comprising about 93.7% of a mixture of 3,3-dichloro-1,1,1,2,2-pentafluoropropane and 1,3-dichloro-1,1,2,2,3-pentafluoropropane, and the balance[[of]] methanol, with trace amounts of nitromethane. Those having ordinary skill in the art will select ~~the~~ a solvent or a mixture of solvents suitable for ~~a~~ the particular polymer being dissolved.

Please replace the paragraph that begins on page 17, line 1, with the following paragraph:

The therapeutic substance ~~which~~ that can be used in the reservoir layer can include any substance capable of exerting a therapeutic or prophylactic effect for a patient. The therapeutic substance may include small molecule sub-

stances, peptides, proteins, oligonucleotides, and the like. The therapeutic substance ~~could~~ can be designed, for example, to inhibit the activity of vascular smooth muscle cells. It can be directed at inhibiting abnormal or inappropriate migration and/or proliferation of smooth muscle cells to inhibit restenosis.

Please replace the paragraph that begins on page 19, line 14, with the following paragraph:

~~Diazenium diolate type~~ Diazenium-diolate-type nitric oxide donors are adducts of nitric oxide with nucleophilic amines. Diazenium diolates, also known as "NONOates," are highly biologically compatible, and in slightly acidic ~~medium~~ media, they spontaneously release NO. One example of diazenium diolate that can be used is spermine diazenium diolate (SDD).

Please replace the paragraph that begins on page 19, line 18, with the following paragraph:

SDD, also known by its chemical name as 1,3-propanediamine, N-{4-[1-(3-aminopropyl)-2-hydroxy-2-nitrosohydrazino] butyl}-diazen-1-ium-1,2-diolate, is an aliphatic NONOate having the formula NH_2–$(CH_2)_3$–$N[N^+(O)$–$(N^-$–$OH)]$–$(CH_2)_4$–NH–$(CH_2)_3$–NH_2 and is available from Molecular Probes, Inc. of Eugene, Oregon. Alternatively, other ~~diazenium diolate type~~ diazenium-diolate-type NO donors can be used. Some examples of the alternative ~~diazenium diolate type~~ diazenium-diolate-type NO donors that can be conjugated to the PEG blocks of PEG-PCL-PEG include 1-{N-methyl-N-[6-(N-methylammonio)hexyl]amino}diazen-1-ium-1,2-diolate having the formula CH_3–N^+H_2–$(CH_2)_6$–$N(CH_3)$–$N^+(O^-)$=N–O^- (MAHMA-NO), and Z-1-[N-(2-aminoethyl)-N-(2-ammonioethyl)amino]diazen-1-ium-1,2-diolate having the formula O-$N^+[N(CH_2CH_2NH_2)CH_2CH_2N^+H_3]$=N–$O^-$ (DETA-NO). MAHMA-NO and DETA-NO can be obtained from Cayman Chemical Co. of Ann Arbor, Michigan.

Please replace the paragraph that begins on page 20, line 6, with the following paragraph:

> In order to carry out conjugation of SDD to a PEG-PCL-PEG block copolymer, the PEG block of the copolymer can be preliminarily derivatized by tosylation (treatment with tosyl chloride), or alternatively by tresylation (by reacting with tresyl chloride). Tosyl chloride is a derivative of toluene, *para*-toluenesulfonyl chloride, having the formula $CH_3–C_6H_4–SO_2Cl$ (TsCl). The process of PEG-PCL-PEG derivatization can be conducted outside the stent or directly on the stent. The processes of tosylation or tresylation include[[s]] an attack on the terminal hydroxyl of the PEG block and can be illustrated by reactions (III) and (IV), respectively:

Please replace the paragraph that begins on page 21, line 30, with the following paragraph:

> One or both PEG blocks of PEG-PCL-PEG can be modified with SDD according to the process described by reactions (III-V). Those having ordinary skill in the art can determine under which conditions the two-step process of conjugating SDD to PEG-PCL-PEG described by reactions (III-V) can be carried out. The resulting polymeric adduct can be described schematically as Dz-PEG-PCL-PEG (one PEG block is modified) or Dz-PEG-PCL-PEG-Dz (two PEG blocks are modified), where Dz is a fragment derived from SDD.

Please replace the paragraph that begins on page 22, line 3, with the following paragraph:

> The coatings and methods of the present invention have been described with reference to a stent, such as a balloon expandable or self-expandable stent. The use of the coating is not limited to stents, however, and the coating can[[also]] be used with a variety of other medical devices. Examples of the implantable medical device[[,]] that can be used in conjunction with the embodiments of this invention include stent-grafts, grafts (e.g., aortic grafts), artificial heart valves, cerebrospinal fluid shunts, pacemaker electrodes, axius

coronary shunts and endocardial leads (e.g., FINELINE and ENDOTAK, available from Guidant Corporation). The underlying structure of the device can be of virtually any design. The device can be made of a metallic material or an alloy such as, but not limited to, cobalt-chromium alloys (e.g., ELGILOY), stainless steel (316L), "MP35N," "MP20N," ELASTINITE (Nitinol), tantalum, tantalum-based alloys, nickel-titanium alloy, platinum, platinum-based alloys such as, e.g., platinum-iridium alloy, iridium, gold, magnesium, titanium, titanium-based alloys, zirconium-based alloys, or combinations thereof. Devices made from bioabsorbable or biostable polymers can also be used with the embodiments of the present invention.

Please replace the paragraph that begins on page 26, line 7, with the following paragraph:

A first composition can be prepared by mixing the following components:

(a) between about 1.0 mass % and about 15 mass %, for example, about 2.0 mass % PEG-PBT; and

(b) the balance, a solvent blend~~, the blend~~ comprising 1,1,2-~~tricloroethane~~ trichloroethane and chloroform in a mass ratio between[[of]] about 4:1.

Please replace the paragraph that begins on page 27, line 14, with the following paragraph:

A fourth composition can be prepared by mixing the following components:

(a) between about 1.0 mass % and about 15 mass %, for example, about 3.0 mass % PEG-PBT; and

(b) the balance, a solvent blend of 1,1,2-~~tricloroethane~~ trichloroethane and chloroform described above.

Please replace the paragraph that begins on page 28, line 6, with the following paragraph:

> A fifth composition can be prepared by mixing the following components:
>
> (a) between about 1.0 mass % and about 15 mass %, for example, about 2.0 mass % PEG-PBT having about 20 molar % PBT units and about 80 molar % PEG units. (The molecular weight of the PEG units can be about 4,000 Daltons);
>
> (b) between about 1.0 mass % and about 15 mass %, for example, about 2.0 mass % an adduct of the same brand of PEG-PBT with hyaluronic acid; and
>
> (c) the balance, the blend of 1,1,2-tricloroethane and chloroform described above.

Please replace the paragraph that begins on page 28, line 21, with the following paragraph:

> A first composition can be prepared by mixing the following components:
>
> (a) between about 1.0 mass % and about 15 mass %, for example, about 2.0 mass % of a silk-elastin protein ~~block~~ block copolymer; and
>
> (b) the balance, DMAC solvent.

Please replace the paragraph that begins on page 29, line 4, with the following paragraph:

> Silk-elastin protein ~~block~~ block copolymers combine[[the]] repeating blocks of amino acids ~~thus~~ providing the copolymer with the mechanical strength characterizing silk and the flexibility characterizing elastin. Silk-elastin ~~block~~

block copolymer can be obtained from Protein Polymer Technologies, Inc. of San Diego, California. The first composition can be applied onto the surface of a bare 18 mm PENTA stent to form a primer layer as described in Example 1. The primer can contain about 70 μg silk-elastin.

Please replace the paragraph that begins on page 30, line 14, with the following paragraph:

The fourth composition can be applied over the reservoir layer using techniques described above, and dried, e.g., by baking~~, to form a~~ to form an intermediate layer. The intermediate layer can contain about 50 μg silk-elastin.

Please replace the paragraph that begins on page 30, line 17, with the following paragraph:

A fifth composition can be prepared by mixing the following components:

(a) between about 1.0 mass % and about 15 mass %, for example, about 2.0 mass % PEG-PBT having about 20 molar % PBT units and about 80 molar % PEG units~~.~~ (The molecular weight of the PEG units can be about 4,000 Daltons);

(b) between about 1.0 mass % and about 15 mass %, for example, about 2.0 mass % PEG-PBT having about 45 molar % PBT units and about 55 molar % PEG units. The molecular weight of the PEG units can be about 300 Daltons; and

(c) the balance, the blend of 1,1,2-~~tricloroethane~~trichloroethane and chloroform described above.

Please replace the paragraph that begins on page 31, line 5, with the following paragraph:

> The fifth composition can be applied onto the dried reservoir layer to form ~~the~~ a topcoat layer[[,]] using the same spraying and drying techniques, as described above. The topcoat layer can then be annealed by ~~being heated~~ heating to about 80°C for about 30 minutes and then to about 50°C for about 1 hour. The topcoat layer can contain about 100 µg of each kind of PEG-PBT.

Please replace the paragraph that begins on page 31, line 10, with the following paragraph:

> A stent can be coated with a primer layer as described in Example 6. A first composition can be prepared, comprising:
>
> (a) between about 1.0 mass % and about 15 mass %, for example, about 2.0 mass % PEG-PBT having about 45 molar % PBT units and about 55 molar % PEG units. (The molecular weight of the PEG units can be about 300 Daltons);
>
> (b) between about 1.0 mass % and about 15 mass %, for example, about 2.0 mass % EVEROLIMUS;
>
> (c) the balance, the blend of 1,1,2-~~tricloroethane~~ trichloroethane and chloroform described above.

Please replace the paragraph that begins on page 31, line 18, with the following paragraph:

> The composition can contain about 100 µg PEG-PBT, and about 100 µg EVEROLIMUS. The composition can be applied onto the dried primer layer to form the reservoir layer[[,]] using the same spraying technique and equipment used for applying the primer layer, followed by drying, e.g., by baking, as described above.

Please replace the paragraph that begins on page 32, line 1, with the following paragraph:

> A second composition can be prepared by mixing the following components:
>
> (a) between about 1.0 mass % and about 15 mass %, for example, about 2.0 mass % PEG-PBT; and
>
> (b) the balance, the blend of 1,1,2-~~tricloroethane~~ trichloroethane and chloroform described above.

Please replace the paragraph that begins on page 32, line 13, with the following paragraph:

> A stent can be coated with a primer layer as described in Example 6. A first composition can be prepared, comprising:
>
> (a) between about 1.0 mass % and about 15 mass %, for example, about 2.0 mass % PEG-PBT having about 45 molar % PBT units and about 55 molar % PEG units~~.~~ (The molecular weight of the PEG units can be about 300 Daltons);
>
> (b) between about 1.0 mass % and about 15 mass %, for example, about 2.0 mass % EVEROLIMUS;
>
> (c) the balance, the blend of 1,1,2-~~tricloroethane~~trichloroethane and chloroform described above.

Please replace the paragraph that begins on page 33, line 1, with the following paragraph:

> The composition can contain about 100 µg PEG-PBT, and about 100 µg EVEROLIMUS. The composition can be applied onto the dried primer layer to form ~~the~~ a reservoir

layer, using the same spraying technique and equipment used for applying the primer layer, followed by drying, e.g., by ~~baking~~ baking, as described above.

Please replace the paragraph that begins on page 33, line 5, with the following paragraph:

A second composition can be prepared, comprising:

(a) between about 1.0 mass % and about 15 mass %, for example, about 2.0 mass % PEG-PBT having about 45 molar % PBT units and about 55 molar % PEG units~~.~~ (The molecular weight of the PEG units can be about 300 Daltons);

(b) between about 1.0 mass % and about 15 mass %, for example, about 2.0 mass % polyaspirin; and

(c) the balance, the blend of 1,1,2-~~trieloroethane~~ tricloroethane and chloroform described above[[.]].

Please replace the paragraph that begins on page 33, line 12, with the following paragraph:

The second composition can be applied over the reservoir layer using techniques described above, and dried, e.g., by baking, to form an intermediate layer. The intermediate layer can contain about 50 μg PEG-PBT and about 50 μg polyaspirin. The reservoir layer/[[the]]intermediate layer sequence can be repeated 4 times to achieve a total EVEROLIMUS load of about 400 μg and a total polyaspirin load of about 200 μg.

Please replace the paragraph that begins on page 33, line 17, with the following paragraph:

A third composition can be prepared by mixing the following components:

(a) between about 1.0 mass % and about 15 mass %, for example, about 2.0 mass % PEG-PBT having about 45 molar % PBT units and about 55 molar % PEG units~~.~~ (The molecular weight of the PEG units can be about 300 Daltons);

(b) between about 1.0 mass % and about 15 mass %, for example, about 2.0 mass % polyaspirin; and

(c) the balance, the blend of 1,1,2-~~tricloroethane~~ trichloroethane and chloroform described above.

Please replace the paragraph that begins on page 34, line 4, with the following paragraph:

The third composition can be applied onto the dried reservoir layer/[[the]]intermediate layer system to form ~~the~~ a topcoat layer[[,]] using the same spraying and drying techniques as described above. The topcoat layer can then be annealed by being heated to about 80°C for about 30 minutes and then to about 50°C for about 1 hour. The topcoat layer can contain about 100 µg PEG-PBT and about 200 µg polyaspirin.